# Behavioral/Systems/Cognitive

# How Connectivity, Background Activity, and Synaptic Properties Shape the Cross-Correlation between Spike Trains

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Functional interactions between neurons *in vivo* are often quantified by cross-correlation functions (CCFs) between their spike trains. It is therefore essential to understand quantitatively how CCFs are shaped by different factors, such as connectivity, synaptic parameters, and background activity. Here, we study the CCF between two neurons using analytical calculations and numerical simulations. We quantify the role of synaptic parameters, such as peak conductance, decay time, and reversal potential, and analyze how various patterns of connectivity influence CCF shapes. In particular, we find that the symmetry of the CCF distinguishes in general, but not always, the case of shared inputs between two neurons from the case in which they are directly synaptically connected. We systematically examine the influence of background synaptic inputs from the surrounding network that set the baseline firing statistics of the neurons and modulate their response properties. We find that variations in the background noise modify the amplitude of the cross-correlation function as strongly as variations of synaptic strength. In particular, we show that the postsynaptic neuron spiking regularity has a pronounced influence on CCF amplitude. This suggests an efficient and flexible mechanism for modulating functional interactions.

# Introduction

Recordings of multineuron spike trains have revealed significant interdependencies between the firing of different neurons in a population (Zohary et al., 1994; Meister et al., 1995; Alonso et al., 1996; deCharms and Merzenich, 1996; Bair et al., 2001; Kohn and Smith, 2005). Although it is important to identify the role such functional interactions play in neural coding (Abbott and Dayan, 1999; Nirenberg et al., 2001; Nirenberg and Latham, 2003; Averbeck et al., 2006; Schneidman et al., 2006; Pillow et al., 2008), it is also important to understand how they depend on biophysical parameters and network activity (Poliakov et al., 1996, 1997; de la Rocha et al., 2007). For pairs of neurons, functional interactions are quantified by the cross-correlation function (CCF) between their spike trains, which measures how much the firing of one of the two neurons influences the firing of the other at different time lags. Statistically significant crosscorrelations arise from the presence of a direct synaptic connection (Snider et al., 1998; Csicsvari et al., 1998; Barthó et al., 2004; Fujisawa et al., 2008) and/or from common or correlated inputs to the two neurons (Sears and Stagg, 1976; Binder and Powers, 2001; Constantinidis et al., 2001; Türker and Powers, 2001, 2002). The amplitude of the CCF therefore directly depends on

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the properties of the synapses mediating the interactions, but it is also modulated by the activity of the surrounding network (Aertsen et al., 1989; Poliakov et al., 1996; Constantinidis et al., 2001). The shape of the CCF also carries information on the underlying connectivity, yet inferring the circuitry from the CCF is a notoriously difficult problem (Melssen and Epping, 1987; Alonso and Martinez, 1998; Trong and Rieke, 2008). A detailed, quantitative understanding of the influences of synaptic parameters, network activity, and local circuitry on the CCF is therefore necessary for a correct interpretation of CCFs.

The basic influence of the underlying circuit on the shape of the CCF has long been considered at a qualitative level (Moore et al., 1970; Palm et al., 1988). More quantitative studies have been devoted to CCFs induced by a direct synaptic connection (Knox, 1974; Ashby and Zilm, 1982; Fetz and Gustafsson, 1983; Herrmann and Gerstner, 2002; Veredas et al., 2005). Early theoretical studies did not take into account the activity of the surrounding network, and it is only more recently that the effects of background inputs have been assessed using a phenomenological noise model (Herrmann and Gerstner, 2001). For the case of common inputs to the neurons, previous theoretical studies have concentrated on spike-count correlations (de la Rocha et al., 2007; Shea-Brown et al., 2008), and the results for the full CCF appear scarce (Kirkwood and Sears, 1978; Tchumatchenko et al., 2008).

In the present work, we systematically examine how the amplitude and time course of the CCF depend on the synaptic parameters, surrounding network activity, and local connectivity. To this end, we use pairs of integrate-and-fire neurons and represent the activity of the surrounding network by a

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compound, fluctuating background input that sets the baseline firing statistics of the neurons. We first show that the average firing response of a neuron to a given synaptic input strongly depends on the regularity of its firing. We next determine analytically the CCF in various simple microcircuits within a linear approximation. We first consider the two basic situations of a direct synaptic connection and common synaptic inputs to the two neurons. We then show how the results obtained for these two microcircuits can be used to study more complex ones, such as two mutually connected neurons and feedforward inhibition.

# Materials and Methods

*Integrate-and-fire models.* To study the influence of various biophysical parameters on the shape and amplitude of the cross-correlation function between the spike trains of two neurons, we used integrate-and-fire models in which action potentials are generated from the underlying dynamics of the membrane potential (Gerstner and Kistler, 2002). These dynamics are given by the following:

$$c_m \frac{dV}{dt} = -g_m V + g_m \psi(V) - I_{\rm syn}(t), \qquad (1)$$

where the membrane potential V is determined with respect to the resting potential of the cell,  $c_m$  is the membrane capacitance of the neuron,  $g_m$  is the membrane conductance,  $g_m\psi(V)$  is a spike-generating current, and  $I_{syn}$  is the total current elicited by synaptic inputs to the neuron. We used  $c_m = 250$  pF and  $g_m = 25$  nS. These parameters are taken from *in vitro* recordings from layer V neocortical pyramidal (Badel et al., 2008b), with  $g_m$  increased by a factor of 2–3 compared with *in vitro* values, to account for *in vivo*-type synaptic background inputs. We studied two different versions of the integrate-and-fire model.

In the leaky integrate-and-fire (LIF) model,  $\psi(V) = 0$ , there is no spike-generation current, and an action potential (AP) is emitted when the membrane potential crosses a fixed threshold value  $V_{\rm T}$ . The membrane potential is subsequently reset to a value  $V_{\rm R}$ . We did not introduce any refractory period after the emission of an AP. The values used for the threshold and reset were  $V_{\rm T} = 20$  mV and  $V_{\rm R} = 10$  mV.

In the exponential integrate-and-fire (EIF) model, the spikegeneration current is exponential:

$$\psi(V) = \Delta_{\rm T} \exp\left(\frac{V - V_{\rm T}}{\Delta_{\rm T}}\right). \tag{2}$$

Once the membrane potential crosses the threshold  $V_{\rm T}$ , it diverges to infinity in finite time. This divergence represents the firing of an action potential. After the divergence, the membrane potential is reset to a value  $V_{\rm R}$ . The values used in this study were  $V_{\rm T} = 10$  mV and  $V_{\rm R} = 3$  mV. The parameter  $\Delta_{\rm T}$  quantifies the sharpness of the AP initiation. We took here  $\Delta_{\rm T} = 1$  mV, a typical value for pyramidal cells (Badel et al., 2008b).

The LIF model (Lapicque, 1907) presents the advantage of being analytically tractable. However, the absence of spike-generating currents and the fixed threshold for spike emission may induce some differences with the behavior of conductance-based models. The EIF model, in contrast, reproduces in the simplest possible way the spike initiation in Hodgkin–Huxley type models (Fourcaud-Trocmé et al., 2003), the spike sharpness being described in the EIF model with a single parameter  $\Delta_T$ . Moreover, it has been shown recently that the EIF model provides an excellent fit to *in vitro* dynamics of the membrane potential in cortical pyramidal neurons (Badel et al., 2008b), with a fitted value for the spike sharpness of  $\Delta_T = ~1$  mV.

If the neuron receives a constant input current  $I_{syn}(t) = -I_0$ , we find it useful to define the effective rest potential  $\mu = I_0/g_m$  as the value the membrane potential of the neuron would reach in the absence of threshold and spike-generating mechanisms.

*Spike-train statistics and the cross-correlation function.* A spike train is represented as the following time series:

$$n(t) = \sum_{j=1}^{p} \delta(t - t_j), \qquad (3)$$

where  $t_j$  for j = 1, ..., p is the series of spike times ordered in time on the interval [0,T]. It is often useful to work with Fourier transforms  $\tilde{n}(\omega) = F[n]$  of spike trains, the Fourier transform F of a function *f* being defined as follows:

$$\mathbf{F}[f] = \int_{-\infty}^{\infty} f(t)e^{-i\omega t}dt, \qquad (4)$$

so that

$$\tilde{n}(\omega) = \sum_{j=1}^{p} e^{-i\omega t_j}.$$
(5)

The instantaneous firing rate v(t) is defined as follows:  $v(t) = \langle n(t) \rangle$ 

$$v(t) = \langle n(t) \rangle, \tag{6}$$

where the brackets denote averaging over trials. If the firing is stationary,  $\nu(t) = \nu_0$  for all *t*.

For stationary firing, the regularity of the spike train is quantified using the coefficient of variation (CV), defined as follows:

$$CV = \frac{\sqrt{(\Delta t_j - \overline{\Delta t_j})^2}}{\overline{\Delta t_j}},$$
(7)

where  $\Delta t_j = t_j - t_{j-1}$  is the *j*th interspike interval, and the bar denotes averaging over all interspike intervals in the spike train.

The autocorrelation function of a spike train is defined as follows:

$$A(t) = \frac{1}{T\nu_0^2} \int_0^T d\tau \, \langle (n(\tau) - \nu_0)(n(\tau + t) - \nu_0) \rangle. \tag{8}$$

The Fourier transform of A(t),  $\tilde{A}(\omega)$ , is equal to the power spectrum of the spike train. It is given by the following:

$$\langle \tilde{n}(\omega)^* \tilde{n}(\omega') \rangle = 2\pi \nu_0^2 \delta(\omega - \omega') \tilde{A}(\omega) + (2\pi \nu_0)^2 \delta(\omega) \delta(\omega').$$
(9)

The cross-correlation function between the spike trains  $n^{(1)}(t)$  and  $n^{(2)}(t)$  of two neurons is as follows:

$$C(t) = \frac{1}{T\nu_0^{(1)}\nu_0^{(2)}} \int_0^T d\tau \, \langle (n^{(1)}(\tau) - \nu_0^{(1)})(n^{(2)}(\tau+t) - \nu_0^{(2)}) \rangle. \tag{10}$$

The value of C(t) represents the variation of the firing rate of the neuron 2, conditioned on the fact that neuron 1 fires *t* milliseconds earlier. With the normalization adopted here, this variation is expressed as the fraction of the baseline firing rate of neuron 2. Note that the normalization used here is different from the normalization by the geometric mean  $\sqrt{\nu_0^{(1)} \nu_0^{(2)}}$  of the firing rates, commonly used for spike-count correlations (Bair, 2001; Kohn and Smith, 2005; de la Rocha et al., 2007).

The Fourier transform  $\tilde{C}(\omega)$  of C(t), also called the cross-spectrum between neurons 1 and 2 is given by the following:

$$\langle \tilde{n}^{(1)*}(\omega)\tilde{n}^{(2)}(\omega')\rangle = 2\pi\nu_0^{(1)}\nu_0^{(2)}\delta(\omega-\omega')\tilde{C}(\omega) + (2\pi)^2\nu_0^{(1)}\nu_0^{(2)}\delta(\omega)\delta(\omega').$$
(11)

In this study, we determine  $\tilde{C}(\omega)$  analytically and then recover C(t) using the inverse Fourier transform.

*Synaptic inputs*. Synaptic inputs are modeled as transient conductance increases that cause a voltage-dependent inward or outward current flow in the postsynaptic neuron. More precisely, the postsynaptic current (PSC) elicited by a single presynaptic AP at time  $t_0$  is given by the following:

$$i_{\rm syn}(t) = g_{\rm syn}(t - t_0)(V(t) - E_{\rm syn}),$$
 (12)

where  $E_{syn}$  is the synaptic reversal potential, and  $g_{syn}$  is the conductance of a synapse. The time evolution of  $g_{syn}$  after a presynaptic spike is given by a delayed exponential:

$$g_{\rm syn}(t) = \begin{cases} 0 & t < \delta_s \\ g_0 \exp\left(-(t-\delta_s)/\tau_s\right), & t > \delta_s \end{cases}$$
(13)

Here  $g_0$  is the peak conductance, and  $\delta_s$  and  $\tau_s$  are the latency and decay time. Unless otherwise indicated, the values of the synaptic times are  $\delta_s = 1.5$  ms (Markram et al., 1997) and  $\tau_s = 3$  ms (Hestrin, 1993).

The maximum amplitude of the postsynaptic current fluctuates from presynaptic spike to presynaptic spike because of the voltage dependence in Equation 12. Its mean is given by  $(\mu - E_{\rm syn})g_0$ , where  $\mu$  is the effective rest potential of the neuron.  $E_{\rm syn} - \mu$  represents the effective driving force of a synapse with reversal potential  $E_{\rm syn}$  in the presence of fluctuating inputs.

*Background synaptic activity.* Each cortical neuron receives a large number of synapses from other neurons, the typical estimate of this number being of the order of tens of thousands (Braitenberg and Schüz, 1991). *In vivo*, neurons are spontaneously active so that any neuron receives persistent background inputs as a result of the firing of its afferents. To study the effect of this background activity on cross-correlation functions, we represent it as a compound background input to the neurons, as precisely described below.

If the amplitude of each postsynaptic current is small with respect to the threshold for spike generation, a large number of synaptic events is needed to cause the firing of an action potential. In such a situation, the cumulative conductance of many co-occurring synaptic inputs generated from random background activity can be described as a Gaussian random process, the so-called diffusion approximation (Tuckwell, 1988).

More precisely, in the case in which the neuron receives two types of synaptic inputs, excitatory and inhibitory ones, for each type of input, the total conductance attributable to background synaptic activity can be expressed as a sum of a tonic and a fluctuating part as follows:

$$g_{\text{tot}}^{\text{E,I}}(t) = \sum_{\text{synapses}} g_{\text{syn}}^{\text{E,I}}(t)$$
(14)

$$=g_0^{\mathrm{E},\mathrm{I}}+\sigma_g^{\mathrm{E},\mathrm{I}}\eta^{\mathrm{E},\mathrm{I}}(t),\qquad(15)$$

where  $g_0^E$  and  $g_0^I$  are the mean background synaptic conductances, respectively, for the excitatory (E) and the inhibitory (I) synapses,  $\sigma_g^E$  and  $\sigma_g^I$  are the SDs of the background synaptic conductances, and  $\eta^E(t)$  and  $\eta^I(t)$ are Gaussian stochastic processes of zero mean and unit SD. For the sake of analytical understanding, we assume that  $\eta^E$  and  $\eta^I$  are uncorrelated in time, i.e.,  $\eta^E$  and  $\eta^I$  are white-noise processes, although this is generally not the case because of the presence of the nonvanishing synaptic decay times  $\tau_s$ . Including a finite correlation time in the background inputs modifies qualitatively the behavior of the LIF model (Brunel et al., 2001) but not the behavior of the EIF model (Fourcaud-Trocmé et al., 2003) or of cortical neurons *in vitro* (Köndgen et al., 2008).

The total postsynaptic current attributable to the background synaptic inputs is given by the following:

$$I_{\rm syn,tot} = g_{\rm tot}^{\rm E}(t)(V - E_{\rm E}) + g_{\rm tot}^{\rm I}(t)(V - E_{\rm I}), \qquad (16)$$

where  $E_{\rm E}$  and  $E_{\rm I}$  are the reversal potentials of excitatory and inhibitory synapses. This current can be decomposed in a sum of a voltageindependent term and a voltage-dependent term. Within the diffusion approximation, the voltage-independent term is described by a tonic and a fluctuating part as follows:

$$I_{\rm syn} = -I_0 + \sigma \sqrt{c_m g_m} \eta(t), \qquad (17)$$

where the mean  $I_0$  and the SD  $\sigma$  can be expressed in terms of  $g_0^{\text{E}}, g_0^{\text{I}}, \sigma_g^{\text{E}}$ , and  $\sigma_g^{\text{I}}$  and the synaptic reversal potentials  $E_{\text{E}}$  and  $E_{\text{I}}$  (Richardson, 2004). This is the background synaptic current term in Equation 1. Throughout this study, we examine only the stationary situation in which  $I_0$  and  $\sigma$  are constant. Note that  $\sigma$  is expressed in millivolt units. In the absence of firing threshold, the SD of the membrane potential is equal to  $\sigma/\sqrt{2}$ .

The voltage dependent part is simply given by  $(g_0^{\text{E}} + g_0^{\text{I}})V$ , i.e., it has no fluctuating part within the diffusion approximation (Richardson, 2004;

Richardson and Gerstner, 2005). The only effect of the voltagedependent part is thus to modify tonically the membrane conductance of the neuron, in a time-independent manner. We therefore incorporate this effect in the model by setting  $g_m$  to a value larger than typically measured *in vitro* in the absence of background inputs.

*Linear response to synaptic inputs.* To evaluate the cross-correlation function between the spike trains of two neurons, we need to quantify how much a conductance change attributable to a single synapse modifies the instantaneous firing rate of a postsynaptic neuron that is in a stationary state. The current elicited by a synaptic conductance change g(t) is as follows:

$$I(t) = g(t)(V - E_{\rm syn}), \qquad (18)$$

where  $E_{syn}$  is the synaptic reversal potential.

We assume that the amplitude of this postsynaptic current is small so that the resulting variation of the firing rate is small, too, and can be described as a linear variation around the stationary firing rate:

$$\nu(t) = \nu_0 + \int_0^\infty R_n(\tau) g(t-\tau) d\tau.$$
 (19)

Here we have averaged over trials, the conductance variation being identical in all trials;  $\nu_0$  is the baseline firing rate attributable to tonic background inputs, and  $R_n$  is the linear response kernel to a synaptic conductance variation. A similar technique was used previously (Lindner et al., 2005). The linear response approximation can be written in frequency as follows:

$$\tilde{\nu}(\omega) = 2\pi\nu_0\delta(\omega) + \tilde{R}_n(\omega)\tilde{g}(\omega), \qquad (20)$$

where  $\tilde{R}_n = F[R_n]$  is the linear response in frequency, and  $\tilde{g} = F[g]$ .

The postsynaptic current in Equation 18 can be decomposed in a sum of two components, a component  $-g(t)E_{syn}$  independent of the membrane potential of the postsynaptic cell, and a component g(t)V proportional to the membrane potential and equivalent to a variation of the membrane conductance. Correspondingly, the linear response to a synaptic input can therefore be expressed as follows:

$$R_n(t) = R_{\rm E}(t)(E_{\rm syn} - \mu) + R_{\rm shunt}(t), \qquad (21)$$

where  $R_{\rm E}$  is the linear response kernel to a variation of the input current to the postsynaptic cell,  $\mu$  is the effective rest potential of the neuron, and  $R_{\rm shunt}$  is the linear response kernel to a variation of its membrane conductance. Equivalently, for the response in frequency, we write  $\tilde{R}_n = \tilde{R}_{\rm E}(E_{\rm syn} - \mu) + \tilde{R}_{\rm shunt}$ .

 $\tilde{R}_{\rm E}(E_{\rm syn} - \mu) + \tilde{R}_{\rm shunt}$ . If  $E_{\rm syn}$  is significantly different from  $\mu$ , the total linear response is dominated by  $R_{\rm p}$ :

$$R_n(t) \approx R_{\rm E}(t)(E_{\rm syn} - \mu). \tag{22}$$

The linear response function  $R_{\rm E}$  is closely related to the Wiener kernel of the neuron (Poliakov et al., 1997) and the spike-triggered average (STA) input current (Paninski, 2006) as described in Appendix B. The full linear response kernel  $R_n$  is calculated in Appendix A.

*Dominant timescale approximation for*  $R_n$ . The linear kernel  $R_n$  can be written as follows:

$$R_n(t) = \Theta(t) \sum_{j=1}^{\infty} a_j e^{z_j t} + \text{complex conj.}, \qquad (23)$$

where  $\{a_j\}$  and  $\{z_j\}$  are complex numbers, with  $0 > Re(z_1) > Re(z_2)...$  (for more details, see Appendix C).

The dominant timescale approximation consists in keeping only the long time asymptotic behavior for  $R_n(t)$ , i.e., the exponential of the pole  $z_1$  with the least negative real part. If the SD  $\sigma$  of the background noise term is small, the dominant pole has a nonzero imaginary part, and we write it as  $z_1 = -1/\tau_1 + i\omega_0$ . In the dominant pole approximation,  $R_n$  becomes as follows:

$$R_n(t) = 2a_1 e^{-t/\tau_1} \cos\left(\omega_1 t\right) \Theta(t).$$
(24)

If  $\sigma$  is larger than a critical value,  $z_1$  becomes real, and we write it as  $z_1 = -1/\tau_1$ , so that in the dominant pole approximation, the following holds true:

$$R_n(t) = 2a_1 e^{-t/\tau_1} \Theta(t).$$
 (25)

# Results

# Firing-rate responses to current and conductance variations

The cross-correlation function between the spike trains of two neurons quantifies the average temporal variation of the firing rate of one neuron relatively to the firing time of the other neuron (Perkel et al., 1967). This variation of the firing rate around its baseline value is ultimately attributable to synaptic inputs, arising for example from a direct synapse between the two neurons or from common or correlated inputs to the two neurons. To describe the cross-correlation function in any circuit, one thus first needs to quantify the effect of a change of its input synaptic conductance on the firing rate of a neuron. It is important to note that the average response to a given synaptic input depends on the baseline state of the neuron, i.e., its baseline firing rate  $\nu_0$  but also the regularity of this firing as quantified by its CV. These properties of the baseline state are set by the background synaptic inputs to the neuron. We therefore systematically examine the influence of stationary background inputs (see Materials and Methods) on the response properties of the neuron.

If the amplitude of the input conductance variation is small compared with the firing threshold of the neuron-as is often the case when only a subset of presynaptic neurons fires-the corresponding variation of the firing rate is proportional to amplitude of the conductance variation and can be described by the linear response of the firing rate of the neuron to synaptic inputs (see Materials and Methods), i.e., the temporal filter mapping the synaptic conductance variation to a variation of the firing rate. This linear filter can be specified either in time by the firing-rate response function  $R_n$  or in frequency by the Fourier transform of  $R_n$  denoted  $\tilde{R}_n$ . Before studying cross-correlation functions, we describe here the properties of  $R_n$  and  $\tilde{R}_n$  for two models of neurons, leaky integrate-and-fire and exponential integrate-and-fire, in the presence of background synaptic noise that induces a baseline firing specified by its frequency  $v_0$  and CV. To disentangle the influence on the response of the baseline firing rate  $v_0$  and baseline firing regularity, while varying the SD  $\sigma$  of background noise, we systematically adjust the mean input to keep  $v_0$  constant. Increasing  $\sigma$  then results in increasing the CV at fixed firing rate (Fig. 1D).

The response function  $R_n$  can be written as follows:

$$R_n = R_{\rm E}(E_{\rm syn} - \mu) + R_{\rm shunt}, \qquad (26)$$

where  $\mu$  is the effective rest potential,  $R_{\rm E}$  is the firing-rate response to a varying input current, and  $R_{\rm shunt}$  is the response to a variation of the membrane conductance (for additional details, see Materials and Methods). If the synaptic reversal potential  $E_{\rm syn}$  is sufficiently different from the effective rest potential  $\mu$ , i.e., if  $E_{\rm syn} - \mu$  is large, the response function  $R_n$  to a synaptic input is essentially equivalent to the response to a varying input current  $R_{\rm E}$ . Conversely, if  $E_{\rm syn}$  is close to  $\mu$ , then  $R_n$  depends strongly on the response  $R_{\rm shunt}$  to a variation of the membrane conductance. We therefore describe  $R_{\rm E}$  and  $R_{\rm shunt}$  separately in the following.

# Response to current modulations

The linear response function  $\bar{R}_{\rm E}$  to input current modulations of different frequencies has been studied theoretically (Brunel et al., 2001; Fourcaud-Trocmé et al., 2003; Richardson, 2007) and experimentally (Köndgen et al., 2008; Boucsein et al., 2009), whereas its equivalent in time  $R_{\rm E}$  is closely related to the Wiener

kernel (Poliakov et al., 1997) and the STA current of the neuron (Paninski, 2006; Badel et al., 2008a) (see Appendix).

For both LIF and EIF models, the response  $\tilde{R}_{\rm E}$  to modulated current is essentially a low-pass filter, the cutoff frequency of which decreases with increasing background synaptic noise. For low background synaptic noise (CV  $\leq 0.5$ ),  $\tilde{R}_{\rm E}(\omega)$  displays resonances at frequencies multiple of the underlying baseline firing frequency  $\nu_0$  (Fig. 1A), and the response in time  $R_E(t)$  displays oscillations at a frequency equal to the baseline firing frequency  $\nu_0$  (Fig. 1*C*). Qualitatively, in this regime in which the neuron spikes regularly with a period T, the effect of a given input at time  $t_0$  is to shift the times of the following spike emissions. Specifically, for the LIF and EIF neurons, an excitatory input advances the next spike, especially when this spike follows closely the input arrival. The effect is to increase the probability of spike emission at the input time  $t_0$  and, because spikes are emitted regularly, also at times that follow it by an integer number of periods  $(t_0 + T,$  $t_0 + 2T,...$ ). Correlatively, between these regularly spaced times when probability of spike emission is increased, the differential shift of spike time by the input decreases the probability of spike emission. For high background noise (CV  $\geq 0.5$ ),  $\tilde{R}_{\rm E}(\omega)$ is instead a pure low-pass filter with a cutoff frequency of the order of  $\nu_0$ , and  $R_{\rm E}(t)$  decays monotonically (Fig. 1*C*). Qualitatively, for high background noise, an excitatory input at time  $t_0$  simply increases the probability of spike emission in a time range after  $t_0$ .

The time course of  $R_{\rm E}$  at short times is determined by the asymptotic behavior of  $\tilde{R}_{\rm E}$  at high frequencies. For the leaky integrate-and-fire model, the amplitude of  $\tilde{R}_{\rm E}$  decays asymptotically as  $1/\sqrt{\omega}$  (Brunel and Hakim, 1999), so that  $R_{\rm E}$  diverges as  $1/\sqrt{t}$  in the limit  $t \rightarrow 0$  (Paninski, 2006). This divergence implies that the LIF model is capable of responding fast to current variations. In contrast, for the exponential integrate-and-fire model, the amplitude of  $\tilde{R}_{\rm E}$  decays asymptotically as 1/w (Fourcaud-Trocmé et al., 2003), so that  $R_{\rm E}$  reaches a finite limit at zero times (Fig. 1*C*). The response of the EIF model is therefore slower at short times than the response of the LIF model.

The asymptotic behavior of  $R_{\rm E}(t)$  at long times can be described using the dominant mode approximation (see Materials and Methods and Appendix C). For high background noise, this approximation predicts that  $R_{\rm E}(t)$  decays exponentially with a time constant  $\tau_1$  that can be calculated from Equation 49 (Appendix B). This time constant determines the longest timescale in the dynamics of the firing rate and sets a limit on the rate of variation of the firing frequency in response to a varying input current. Interestingly, the value of  $\tau_1$  depends on the input statistics, i.e., on the SD of the background noise  $\sigma$  and the baseline firing frequency  $\nu_0$  of the neuron. In Figure 1 F, the time constant  $\tau_1$  is displayed as a function of the SD of background noise  $\sigma$ , the firing rate  $v_0$  being held constant by adjusting the mean background input while  $\sigma$  is varied. For the LIF model,  $\tau_1$  increases with  $\sigma$ , whereas for the EIF model, it reaches a maximum at intermediate values of  $\sigma$  and decreases for larger values of  $\sigma$ . In both models,  $\tau_1$  decreases with increasing  $\nu_0$ . In particular, it appears to be always smaller than the membrane time constant  $\tau_m$ .

The amplitude  $\sigma$  of the background noise strongly modulates the amplitude of the response and affects differently the response at low and high frequencies. The response  $\tilde{R}_E$  at low frequencies is given by the gain of the neuron, i.e., the variation of its background firing rate when its mean input current is changed. The gain of a neuron is known to depend on the amplitude of background noise (Chance et al., 2002). Figure 1*E* shows that,



**Figure 1.** Neuronal firing rate response to varying input current, for the leaky integrate-and-fire model (left column) and the exponential integrate-and-fire model (right column). *A*, Modulus of the response  $R_E$  as function of input frequency for two values of background noise corresponding to regular firing (CV = 0.2; LIF,  $\sigma$  = 0.5 mV; EIF,  $\sigma$  = 1 mV) and irregular firing (CV = 0.8; LIF,  $\sigma$  = 6 mV; EIF,  $\sigma$  = 8 mV). The dashed line represents the asymptotic decay at large frequencies. *B*, Phase of  $\tilde{R}_E$ . *C*, Response in time  $R_E(t)$ , for the two values of background noise. The dashed line represents the dominant time approximation  $2a_1 \exp(-t/\tau_1)$  in the case of large noise. *D*, CV of the interspike intervals as function of the SD  $\sigma$  of background synaptic noise. *E*, Gain as function of  $\sigma$ . The gain is defined as a the value of  $\tilde{R}_E$  at zero frequency. It corresponds to the slope of the *f*-*l* curve of the neuron at firing rate  $v_0$  and given level of background noise  $\sigma$ . *F*, Dominant decay time  $\tau_1$  as function of  $\sigma$ . In *A*-*C*, the firing rate is 30 Hz. In *D*-*F*, the baseline firing rate is maintained constant by adjusting the mean input current as  $\sigma$  is varied.

for both models studied, the gain decreases with increasing  $\sigma$ , the magnitude of this variation being dependent on the baseline firing rate  $\nu_0$ . The effect of noise on the amplitude of the response at high frequencies is different from its effect on the gain but depends on the model: for the LIF model,  $\tilde{R}_{\rm E}(\omega)$ scales as  $1/\sigma$  for large  $\omega$ , whereas for the EIF model, it is independent of  $\sigma$  (Fourcaud-Trocmé et al., 2003).

#### *Response to membrane conductance modulations*

If the synaptic reversal potential  $E_{syn}$  is close to the effective rest potential  $\mu$  of the neuron, the membrane conductance variation after a synaptic input plays an important role in the firing rate response. In particular, if  $E_{syn}$  is exactly equal to the effective rest potential  $\mu$ , then the firing rate response is entirely attributable to shunting, i.e.,  $\tilde{R}_n = \tilde{R}_{shunt}$ . The influence of the variation of membrane conductance on the firing response can be understood in the LIF model as a superposition of two effects, a variation of the membrane timescale of the neuron, and a variation of the amplitude of the fluctuating input (for details, see Appendix A). These two effects compete against each other: increasing the conductance decreases the effective time constant, leading to an instantaneous increase of the firing rate, but it also decreases the effective level of noise, the effect of which depends on whether the mean input is subthreshold ( $\mu$  below the threshold  $V_T$ ) or suprathreshold ( $\mu > V_T$ ). In the case of subthreshold input, the shunting part  $R_{\rm shunt}$  of the linear response in time  $R_n$  is biphasic, with a fast negative part and a slower positive part. In contrast, for suprathreshold inputs,  $R_n$  is positive at all times. These two cases are illustrated in Figure 2, where  $\nu_0 = 30$  Hz corresponds to a subthreshold input.

In summary, in this section, we have examined the firing-rate response of a neuron to a time-varying conductance input. We have shown that both the amplitude and the timescales of this response strongly depend on the baseline firing statistics of the neuron, set by the background synaptic input.



**Figure 2.** Linear response of the instantaneous firing rate of an LIF neuron to a membrane conductance variation, in the case of subthreshold inputs ( $\nu_0 = 30$  Hz) and suprathreshold inputs ( $\nu_0 = 65$  Hz). *A*, Modulus of the response  $\bar{R}_{\rm shunt}$  to different input frequencies. *B*, Phase of  $\bar{R}_{\rm shunt}$ . *C*, Linear response in time,  $R_{\rm shunt}(t)$ . The SD of background noise is  $\sigma = 6$  mV.

## Correlations arising from a direct synaptic connection

Having characterized the response of a neuron to synaptic inputs, we now turn to the cross-correlation function between spike trains of two neurons arranged in different circuits. We first examine the cross-correlations attributable to a direct synaptic connection between two neurons (Fig. 3). Assuming that both the presynaptic and the postsynaptic neuron receive background synaptic inputs uncorrelated from each other, the crossspectrum can be expressed as follows:

$$\tilde{C}(\omega) = \frac{\nu_0^{(\text{pre})}}{\nu_0^{(\text{post})}} \tilde{R}_n(\omega) \tilde{g}_{\text{syn}}(\omega) \tilde{A}_{\text{pre}}(\omega), \qquad (27)$$

where  $\tilde{R}_n$  is the linear response function of the postsynaptic neuron (see previous section) (Figs. 1, 2),  $\tilde{g}_{syn}$  is the Fourier transform of the synaptic conductance time course after a single presynaptic spike (see Materials and Methods),  $\tilde{A}_{pre}(\omega)$  is the power spectrum of the spike train of the presynaptic neuron, and  $\nu_0^{(pre)}$ (resp.  $\nu_0^{(post)}$ ) is the stationary firing rate of the presynaptic (resp. postsynaptic) neuron. Details of the derivation are provided in Appendix D.

Because  $\tilde{R}_n = \tilde{R}_{\rm E}(E_{\rm syn} - \mu) + \tilde{R}_{\rm shunt}$ , the cross-correlation function can be written as  $C(t) = C_{\rm E}(t) + C_{\rm shunt}(t)$ , with  $C_{\rm E}(t)$  purely induced by current variations and proportional to the amplitude  $g_0(E_{\rm syn} - \mu)$  of the postsynaptic current and  $C_{\rm shunt}(t)$ 

purely induced by membrane conductance variations and proportional to the peak synaptic conductance  $g_0$ . If  $E_{syn} - \mu$  is large enough,  $C_{shunt}(t)$  is negligible with respect to  $C_E(t)$ . We therefore first examine current-induced cross-correlations and later examine the influence of conductance variations for  $E_{syn}$ close to  $\mu$ . Note that  $C_E(t)$  is proportional to  $(E_{syn} - \mu)$ , the sign of which determines whether the synapse is excitatory or inhibitory.

#### Poisson presynaptic firing

It is instructive to consider first the situation in which the firing of the presynaptic neuron is a Poisson process, in which case the power spectrum  $\tilde{A}_{pre}(\omega)$  is a constant. The cross-correlation function  $C_{\rm E}(t)$  is then simply given by the synaptic conductance time course filtered through the linear response function  $R_n$ . In particular,  $C_{\rm E}(t)$  at negative times is necessarily zero, and a nonzero synaptic delay  $\delta_s$  simply shifts  $C_{\rm E}(t)$  by  $\delta_s$  to positive times.

Because  $R_{\rm E}$  filters out high frequencies (Fig. 1*A*,*B*), the time course of current-induced cross-correlations is always slower than the time course of the postsynaptic current (Fig. 3*A*,*B*). For low background noise (Fig. 3*A*), the resonances in  $\tilde{R}_{\rm E}$  (Fig. 1*A*) lead to secondary peaks at positive times in the cross-correlation function  $C_{\rm E}(t)$ , located at multiples of the baseline firing frequency  $\nu_0$ . For high background noise,  $C_{\rm E}(t)$  displays a single peak as shown in Figure 3*B*. In that case, within the dominant timescale approximation, the cross-correlation function can be expressed as a difference of two exponentials:

$$C_{\rm E}(t) = C_0 \frac{\tau_{\rm s} \tau_1}{(\tau_{\rm s} - \tau_1)} \left[ \exp\left(-\frac{t - \delta_{\rm s}}{\tau_{\rm s}}\right) - \exp\left(-\frac{t - \delta_{\rm s}}{\tau_1}\right) \right] \quad \text{for} \quad t > \delta_{\rm s}, \quad (28)$$

where  $\delta_s$  and  $\tau_s$  are the latency and the decay time of the synaptic conductance,  $\tau_1$  is the dominant timescale in  $R_n(t)$  (Fig. 1C), and  $C_0$  is a constant given in Appendix C. Figure 3B shows that the dominant mode approximation describes well the asymptotic decay of  $C_{\rm F}(t)$  at large times, the timescale of that decay being given by the maximum between the neuronal timescale  $\tau_1$  and the synaptic timescale  $\tau_s$  as seen from Equation 28. The dominant approximation, however, fails to describe the small time behavior of  $C_{\rm F}(t)$ , which is determined by the fast components of  $R_{\rm F}(t)$  at small t. The main difference between the LIF and the EIF model is that, for the LIF model,  $R_{\rm E}$  diverges at small t, which leads to a fast rise of  $C_{\rm E}(t)$  at small t, whereas in the EIF model,  $R_{\rm E}$  remains finite and correspondingly the rise  $C_{\rm E}(t)$  at small t is slower. Despite this qualitative difference at short times, the CCFs for the two models end up looking very similar (Fig. 3, compare both *B* panels). This is in part attributable to the fact that, for the values of the noise used in Figure 3*B*, the dominant timescale  $\tau_1$  is very similar in both models.

The peak time and amplitude of the cross-correlation function  $C_{\rm E}(t)$  naturally depend on the biophysical parameters of the synaptic connection, its peak conductance  $g_0$ , and decay timescale  $\tau_{\rm s}$ . Because we are using a linear approximation, the amplitude of  $C_{\rm E}(t)$  is proportional to  $g_0$ . In Figure 4, we examine the accuracy of the linear approximation by comparing our theoretical predictions with numerical simulations for different values of the PSC amplitude  $g_0(\mu - E_{\rm syn})$ . The level of accuracy of the linear approximation depends on the ratio between the PSC amplitude and the noise amplitude: for high noise, the approximation is excellent over a wide range of physiological PSC ampli-



**Figure 3.** Cross-correlation function C(t) arising from a direct synaptic connection between the two neurons, in the case of current-dominated inputs ( $E_{syn} - \mu \gg 1$ ). The presynaptic neuron is a Poisson process and the postsynaptic neuron an LIF (left column) or an EIF (right column). **A**, Time course of the cross-correlation function C(t) for low background synaptic noise, corresponding to a CV of 0.2 (LIF,  $\sigma = 0.5$  mV, PSC amplitude of 15 pA; EIF,  $\sigma = 1$  mV, PSC amplitude of 25 pA). For comparison, the time course of the postsynaptic current is shown in orange (rescaled in arbitrary units). The histogram displays results of direct numerical simulations. **B**, Same as in **A**, in the case of high background synaptic noise, corresponding to a CV of 0.8 (LIF,  $\sigma = 6$  mV, PSC amplitude of 100 pA; EIF,  $\sigma = 8$  mV, PSC amplitude of 125 pA). The dashed trace shows the dominant timescale approximation for C(t). In **A** and **B**, the baseline firing rate of the postsynaptic neuron is 30 Hz. **C**, **D**, Peak value and peak time of C(t), as function of the synaptic decay time  $\tau_{s_1}$  for CV = 0.8. **E**, **F**, Peak value (log scale) and peak time of C(t), as function of the SD  $\sigma$  of background synaptic noise. While varying  $\sigma$ , the firing rate  $v_0$  (10, 30, and 50 Hz as described by the legend in **E**). The synaptic decay time was  $\tau_s = 3$  ms, except in **C** and **D**. The amplitude of the postsynaptic current was 60 pA (corresponding to a peak postsynaptic potential of 0.5 mV), except in **A** and **B**.

tudes; in contrast, for low noise, deviations are seen for large PSCs. Note that the linear approximation does not capture the asymmetry between inhibitory and excitatory CCFs, as pointed out previously (Herrmann and Gerstner, 2001).

Because the cross-correlation function is a filtered version of the synaptic conductance time course, its peak time and amplitude increase with  $\tau_s$  as seen in Figure 3, *C* and *D*. For fixed  $g_0$ , longer-lasting postsynaptic currents thus have a stronger effect on the firing of the postsynaptic neuron. Such a dependence is qualitatively described by the dominant timescale approximation (see Appendix D), although this approximation is not very accurate quantitatively.

The peak time and amplitude of the cross-correlation function are not set by the synaptic properties alone but depend strongly on the statistics of baseline firing of the postsynaptic neuron. The effect of the background synaptic noise amplitude is shown in Figure 3*E*. The neuron firing rate is kept fixed by adjusting the mean input so that only its CV varies with the noise amplitude. Remarkably, one sees that, for the LIF model, the cross-correlation amplitude decreases inversely proportionally to the SD  $\sigma$  of the background noise. In other words, the regularity of the baseline firing of the postsynaptic neuron has a strong influence on the amplitude of the cross-correlations: for a given synaptic peak conductance and decay time, the more regularly the postsynaptic neuron fires, the larger the cross-correlation amplitude. This is also true for the EIF model, although in that model the modulation of the cross-correlation amplitude with noise strength is somewhat weaker, as shown in Figure 3*E*. For



**Figure 4.** Testing the validity of the linear approximation in the case of a direct synaptic connection between two LIF neurons: the theoretical predictions based on the linear approximation (black traces) are compared with numerically estimated cross-correlation functions, obtained by varying the amplitude  $g_0(E_{syn} - \mu)$  of the PSC (color scale). On the vertical axis, the CCF amplitude is rescaled by the PSC amplitude  $g_0(E_{syn} - \mu)$ . Left, Low noise, CV = 0.2,  $\sigma = 0.5$  mV; right, high noise, CV = 0.8,  $\sigma = 6$  mV. The color scale is the same in both panels, and the firing rate is 30 Hz. The insets display the amplitude of the CCF as function of the PSC amplitude compared with the linear prediction (black line).

both models, the cross-correlation amplitude decreases with increasing baseline firing rate  $\nu_0$ , but varying  $\nu_0$  modulates the cross-correlation amplitude in a weaker manner than varying  $\sigma$ . Conversely, the peak time of C(t) is relatively insensitive to  $\sigma$ , for both LIF and EIF models. The peak time decreases with increasing firing rate, in agreement with the predictions of the dominant timescale approximation.

For the sake of comparison with experimental studies, in Figure 3, C and E, the peak value of the cross-correlation function is given for a synaptic conductance corresponding to a postsynaptic current amplitude of 60 pA and a synaptic decay time  $\tau_s = 3$  ms, yielding a postsynaptic potential (PSP) peak of 0.5 mV, a typical order of magnitude for AMPA-dependent EPSPs in the cortex (Markram et al., 1997; Sjöström et al., 2001; Holmgren et al., 2003; Barbour et al., 2007). For background synaptic inputs corresponding to a firing rate  $\nu_0 = 30$  Hz and CV = 0.9 ( $\sigma = 8$  mV in the LIF model), our analysis predicts a corresponding peak cross-correlation of 0.15, meaning that the synaptic inputs from the presynaptic neuron increase the firing rate of the postsynaptic neuron by 15% with respect to the baseline firing rate. If the background noise amplitude is reduced by half to  $\sigma = 4$  mV, the CV becomes 0.7, but the amplitude of the cross-correlations increases to 0.3.

#### Influence of the firing statistics of the presynaptic neuron

If the firing of the presynaptic neuron is not poissonian, the autocorrelation of the presynaptic firing also plays a role in the cross-correlation function (see Eq. 27). We examined the effect of the presynaptic autocorrelation for the LIF models, for which the power spectrum  $\tilde{A}_{pre}(\omega)$  can be analytically calculated (see Appendix E). Depending on the level of background synaptic noise, the LIF neuron can be found in one of the three following regimes, illustrated in Figure 5A: (1) for weak background noise (CV < 0.5), the neuron fires rhythmically, and its autocorrelation function exhibits peaks at multiples of the mean interspike interval; (2) for intermediate background noise (0.5 < CV < 1), the presynaptic neuron fires irregularly but exhibits a noisedependent refractory period around zero in the autocorrelation function; (3) for strong background noise (CV > 1), the neuron tends to fire in bursts, which results in positive autocorrelation at short time lags. The effect of the presynaptic autocorrelation on the cross-correlation function is most prominent at negative times (corresponding to the postsynaptic neuron firing before the presynaptic one), in which C(t) is essentially given by the

autocorrelation function of the presynaptic neuron. This is illustrated in Figure 5B in the three firing regimes of the presynaptic neuron. For weak noise in the presynaptic neuron, C(t) displays periodic secondary peaks at both positive and negative times, corresponding to the period T in the firing of the presynaptic neuron. The peaks correspond to increased postsynaptic spiking arising from the spikes at (..., -2T, -T, 0, T, 2T, ...) in the presynaptic neuron. For intermediate noise in the presynaptic neuron, regular spiking disappears and C(t) simply displays a dip close to zero attributable to the refractory period of the presynaptic neuron. For strong noise in the presvnaptic neuron, C(t) displays positive values close to zero as a result of the bursts in the presynaptic neuron. It is important to note

that the firing statistics of the presynaptic neuron affect only marginally the amplitude of the cross-correlation function, in contrast to the firing statistics of the postsynaptic neuron. Interestingly, the amplitude of the CCFs increase when presynaptic CV increases, whereas it decreases when postsynaptic CV increases. Figure 5*C* displays the effect of the presynaptic firing rate on C(t) at intermediate presynaptic noise: the effect of the presynaptic refractory period increases with increasing presynaptic firing rate.

#### Shunting effects

If the synaptic reversal potential  $E_{syn}$  is close to the effective resting potential  $\mu$  of the postsynaptic neuron, the membrane conductance variations have an important influence on the crosscorrelation function. Figure 6 displays the total cross-correlation function  $C(t) = C_{\rm E}(t) + C_{\rm shunt}(t)$  for  $E_{\rm syn}$  close to the effective rest potential  $\mu$ . For  $E_{syn} = \mu$ , at the point of crossing between inhibition and excitation, the full cross-correlation is given by C<sub>shunt</sub>. If the input is subthreshold ( $\mu < V_T$ ),  $R_{shunt}$  is biphasic, so that C(t) is biphasic with a fast inhibitory phase at small times and a slower excitatory phase at long times (Fig. 6A). For  $E_{syn}$  close to  $\mu$ , depending on the sign of  $E_{\rm syn} - \mu$ , the excitatory or inhibitory phase of  $C_{\text{shunt}}(t)$  is amplified by the cross-correlation  $C_{\text{E}}(t)$  arising from current variations. For  $E_{\rm syn} - \mu$ , negative but small  $C_{\rm E}(t)$  approximately cancels the slow excitatory phase of  $C_{\rm shunt}$ , and only the fast inhibitory part of  $C_{\text{shunt}}$  remains in C(t). Note that this inhibitory part is as fast as the postsynaptic current and thus significantly faster than cross-correlations arising from current variations alone.

If the input is suprathreshold,  $R_{\text{shunt}}$  is monophasic, and  $C_{\text{shunt}}(t)$  is purely excitatory for  $E_{\text{syn}} = \mu$ . C(t) becomes biphasic when the effective resting potential  $\mu$  is slightly below the synaptic reversal potential (Fig. 5*C*) arising from a competition between an excitatory shunting effect and an inhibitory effect arising from the negative effective driving force. The average background level at which the transition between an excitatory and an inhibitory CCF occurs thus depends on the baseline firing rate.

If the effective driving force  $E_{\text{syn}} - \mu$  is of the order of tens of millivolts, current variations dominate, and shunting hardly affects the amplitude of C(t). However, it modifies the time course of C(t) with respect to the CCF  $C_{\text{E}}(t)$  purely induced by current variations: the time course of C(t) is faster than that of  $C_{\text{E}}(t)$  in



**Figure 5.** Effect of the autocorrelation of presynaptic firing on the cross-correlation function C(t) in the case of a direct synaptic connection between the neurons. Both neurons are LIF neurons, receiving independent background inputs with different statistics. *A*, Autocorrelation function of the presynaptic spike train for low, intermediate, and high background noise. *B*, Corresponding cross-correlation function C(t) compared with C(t) obtained for a poissonian presynaptic spike train. The postsynaptic neuron receives an intermediate level (CV = 0.8,  $\sigma = 6$  mV) of synaptic noise, and both neurons are firing at a stationary rate of 30 Hz. *C*, C(t) for three different values of the presynaptic firing rate  $\nu_{pre'}$  for moderate background noise in both neurons ( $\sigma = 6$  mV). The anti-correlations at negative times increase with  $\nu_{pre'}$ . In *B* and *C*, the PSC amplitude is 30 pA.

the case of inhibition and slower in the case of excitation. This is illustrated in Figure 6*B* for subthreshold inputs and  $E_{\text{syn}} - \mu = 10 \text{ mV}$  and in Figure 6*D* for suprathreshold input and  $E_{\text{syn}} - \mu = 30 \text{ mV}$ .

To summarize, we have shown that the primary peak in the cross-correlation function arising from a synaptic connection corresponds to a filtered postsynaptic current. The amplitude and the shape of this peak therefore depend on the peak postsynaptic current and decay time of the corresponding synapse. However, these amplitude and shape are not determined by synaptic properties alone but are strongly modulated by the baseline firing statistics of the postsynaptic neuron and in particular the regularity of its firing. Conversely, the firing statistics of the presynaptic neuron only have a minor effect on correlations at short times. Finally, if the synaptic reversal potential is close to the effective rest potential of the postsynaptic neuron, shunting effects can either accelerate (in the case of inhibition) or slow down (in the case of



**Figure 6.** Effects of shunting on the cross-correlation function for an LIF model. **A**, Cross-correlation function C(t) arising from a direct synaptic connection, in the case when the synaptic reversal potential is close to the effective rest potential  $\mu$  of the postsynaptic cell. For  $E_{syn} = \mu$ , the cross-correlation function is a result of shunting alone. **B**, Comparison between the full cross-correlation function C(t) (solid lines) and the cross-correlations  $C_{\rm E}$  resulting from current inputs (dashed line). Shunting accelerates the cross-correlation function in the case of inhibition and delays it in the case of excitation. In **A** and **B**, the mean input is subthreshold, with  $\nu_0 = 30$  Hz and  $\sigma = 6$  mV. **C**, **D**, Same as in **A** and **B**, but for a suprathreshold input ( $\nu_0 = 65$  Hz and  $\sigma = 6$  mV). In all panels,  $g_0 = 8$  nS.

excitation) the time course of the cross-correlation function.

#### Correlations arising from common inputs

Correlations between the spike trains of two neurons can be induced by common or correlated inputs to the two neurons, even in the absence of a direct synaptic connection between them (Sears and Stagg, 1976; Binder and Powers, 2001; Türker and Powers, 2001, 2002; de la Rocha et al., 2007; Shea-Brown et al., 2008; Tchumatchenko et al., 2008). Assuming that the two neurons, labeled 1 and 2, receive a spike train  $n_{\rm pre}$  from  $N_{\rm pre}$  common presynaptic neurons on top of other uncorrelated background inputs (Fig. 7A), the cross-spectrum between neurons 1 and 2 can be expressed as follows:

$$\tilde{C}(\omega) = \frac{(\nu_0^{(\text{pre})})^2}{\nu_0^{(1)}\nu_0^{(2)}} (\tilde{R}_n^{(1)}(\omega)\tilde{g}_{\text{syn}}^{(1)}(\omega))^* (\tilde{R}_n^{(2)}(\omega)\tilde{g}_{\text{syn}}^{(2)}\omega)\tilde{A}_{\text{pre}}(\omega),$$
(29)

where  $\tilde{R}_n^{(1)}$  and  $\tilde{R}_n^{(2)}$  are the linear response functions of the neurons 1 and 2,  $\tilde{g}_{\rm syn}^{(1)}$  and  $\tilde{g}_{\rm syn}^{(2)}$  are the Fourier transforms of the synaptic conductance time courses in the two neurons after a single presynaptic spike, and  $\nu_0^{\rm (pre)}$  and  $\tilde{A}_{\rm pre}(\omega)$  are the stationary rate



**Figure 7.** Cross-correlation function C(t) arising from common inputs to the two neurons. The two neurons are identical LIF (left column) or EIF (right column) neurons, receiving common inputs in addition to independent background niputs with identical statistics. **A**, Time course of the cross-correlation function C(t) for a low level of background noise [CV = 0.2; LIF,  $\sigma = 0.5 \text{ mV}$ ; EIF,  $\sigma = 1 \text{ mV}$ ;  $g_0(E_{syn} - \mu)N_{pre} = 10 \text{ pA}$ ], both neurons firing at 30 Hz. The histogram displays results of direct numerical simulations. **B**, Same as in **A**, for a high level of background noise [CV = 0.8; LIF,  $\sigma = 6 \text{ mV}$ ; EIF,  $\sigma = 8 \text{ mV}$ ;  $g_0(E_{syn} - \mu)N_{pre} = 10 \text{ pA}$ ]. The blue trace shows C(t) obtained by keeping only the dominant timescale  $\tau_1$  in the firing-rate response. This approximation describes the asymptotic decay of the cross-correlation function C(t). **C**, Amplitude of the peak of C(t), as function of the SD  $\sigma$  of background synaptic noise (log scale). While varying  $\sigma$ , the firing rate  $\nu_0$  was kept constant by adjusting the mean input current to both neurons. Results are shown for three different values of the firing rate  $\nu_0$ .

and power spectrum of the activity  $n_{\text{pre}}$  in the common presynaptic network of the two neurons ( $n_{\text{pre}}$  is obtained by superposing the spike trains of all  $N_{\text{pre}}$  neurons in the common presynaptic network). Here we assume that the synaptic properties (reversal potential, peak conductance, and decay time) for each neuron are identical for all inputs from the common presynaptic network. Details of the derivation are provided in Appendix D.

For each neuron, the response function  $\bar{R}_n$  is a sum of a current-dependent term  $\bar{R}_E(E_{syn} - \mu)$  and a conductancedependent term  $\bar{R}_{shunt}$ . We consider only the current-dominated regime in which  $E_{syn} - \mu$  is large so that C(t) is proportional to  $g_0^2(E_{syn} - \mu)^2 N_{pre}^2$  i.e., to the square of the peak PSC of a single synapse, multiplied by the number  $N_{pre}$  of common presynaptic neurons. Within this approximation, inhibitory and excitatory common inputs lead to identical cross-correlations. For  $E_{syn}$  close to the effective rest potential  $\mu$ , the shunting term prevents C(t) from going to zero but does not change the qualitative shape of C(t) (data not shown).

We first examine the cross-correlations resulting from uncorrelated Poisson common inputs, corresponding to constant presynaptic power spectrum  $\tilde{A}_{pre}(\omega) = A_0$  and later discuss the additional effect of synchrony in common inputs.

#### Asynchronous inputs

If the two neurons have identical properties, meaning that their firing statistics and synaptic inputs are identical, Equation 29 predicts that the cross-correlation function C(t) is symmetrical around its maximum. Here we consider only the situation in

which the common inputs reach the two cells simultaneously, in which case the maximum is located at the origin. If the inputs reach the two cells with different delays, the maximum is shifted away from the origin. Figure 7, *A* and *B*, displays the cross-correlation function C(t) in the two cases of low and high back-ground noise. For low background noise (CV = 0.2), C(t) displays a central peak as well as secondary peaks at multiples of the firing period as a result of to the resonance present in  $\tilde{R}_{E}$ . Hence, common stochastic inputs induce oscillatory synchronization between the two neurons. This observation corresponds to the well known phenomenon of noise-induced synchronization (Pikovsky et al., 1997; Ermentrout et al., 2008).

As noise is increased, the amplitude of the secondary peaks decreases, and, for moderately high background noise (CV = 0.8), C(t) has a single central peak. In that case, using the dominant timescale approximation for  $\tilde{R}_{\rm E}$ , the cross-correlation function can be expressed as the difference of two exponentials:

$$C(t) = \frac{C_0}{\tau_s - \tau_1} \left( \tau_s e^{-|t|/\tau_s} - \tau_1 e^{-|t|/\tau_1} \right), \tag{30}$$

where  $\tau_s$  is the decay time of the synaptic conductance,  $\tau_1$  is the dominant timescale in  $R_n(t)$  (Fig. 1*F*), and  $C_0$  is a constant given in Appendix D. As shown in Figure 7*B*, this approximation typically underestimates the peak of C(t) at zero but captures well the decay of C(t), the timescale of which is given by the maximum between the synaptic timescale  $\tau_s$  and the neuronal timescale  $\tau_1$ .

The synaptic parameters of the common inputs have an important influence on the shape and amplitude of the cross-



**Figure 8.** Cross-correlation function *C*(*t*) arising from common inputs, for two LIF neurons with different firing statistics. *A*, Low noise: neuron 1 fires at 30 Hz, and neuron 2 fires at 30 and 100 Hz. The noise amplitude was adjusted so that both neurons fire with CV = 0.2 in the two cases. *B*, High noise: neuron 1 fires at 10 Hz, and neuron 2 fires at 10, 30, and 100 Hz. The noise amplitude was adjusted so that both neurons fire with a CV of 0.8 in all cases. *C*, Varying the CV: neuron 1 fires with a CV of 0.6, whereas neuron 2 fires with CVs of 0.6, 0.8, and 1. The mean firing rate of both neurons is 30 Hz. In the three panels, amplitudes are normalized to unity to facilitate the comparison between the symmetry of the CCFs.

correlation function. The dominant timescale approximation shows that the decay of the cross-correlation function cannot be faster than the timescale  $\tau_s$  of synaptic decay. The amplitude of the cross-correlation function is proportional to the square of the peak synaptic conductance but also depends on the synaptic timescale  $\tau_s$ . Figure 7*C* shows that the peak value of *C*(*t*) increases approximately linearly with  $\tau_s$ , in contrast to the case of correlations generated by a direct synaptic connection between the two neurons, where  $\tau_s$  has a weaker effect on the amplitude of *C*(*t*). Note that this linear trend is not captured by the dominant timescale approximation.

The shape and amplitude of the cross-correlation function are not fully determined by the synaptic properties of common inputs but are again also strongly modulated by the statistics of firing of the two neurons, which are determined by independent background inputs to each of them. In particular, Figure 7D shows that changing the regularity of firing while keeping the firing rate constant strongly modulates the amplitude of the cross-correlation function, the peak of which decreases approximately quadratically with the SD  $\sigma$  of background noise in the LIF model. In the EIF model, the dependence on  $\sigma$  is somewhat weaker but nevertheless important. The amplitude of the crosscorrelation function is also modulated by the baseline firing rate  $\nu_0$  but in a weaker manner. In both LIF and EIF models, the maximum of C(t) decreases with increasing  $\nu_0$ .

## Effects of heterogeneity

The cross-correlation function C(t) is symmetric around the origin as long as all properties of the two neurons are identical. This symmetry is, however, broken if the firing properties (firing rate and coefficient of variation) of the two neurons are different. Figure 8, *A* and *B*, displays the cross-correlation functions for neurons firing at different firing rates but with identical CV compared with the symmetric case. For high background noise, even if heterogeneity is strong (neuron 1 firing at 10 Hz and neuron 2 firing at 100 Hz), the cross-correlation function remains highly symmetric and very close to the homogeneous case. Note that, if the two neurons have different firing thresholds but identical firing rate and CV, the cross-correlation function is perfectly symmetric. For low background noise (Fig. 8*A*), the two different firing rates lead to secondary peaks at different periods on the two sides of the origin. This is a consequence of causality, namely, that an input modifies spiking after its arrival, not before. Qualitatively, observing a spike in neuron 1 at t = 0 increases the probability that an excitatory input has arrived just before t = 0. Because part of the inputs are common to the two neurons, it also increases the probability of a spike in neuron 2 at approximately t = 0 and also subsequently approximately  $(t = T_2, 2T_2,...)$  when neuron 2 is spiking regularly with period  $T_2$ . Because conditioning the firing of neuron 1 on the spikes of neuron 2 amounts to time inversion, the same reasoning explains that, for negative t, the peaks in the correlation function occur at the firing period of neuron 1. The full cross-correlation function is therefore highly asymmetric, although the two neurons receive the same input that arrives with the same delay. Altogether, these results suggest that the symmetry of the cross-correlation function allows for a reliable discrimination between the underlying common inputs and a direct synaptic connection in the case of strong background noise but not in the case of low background noise, the two cases being distinguished by the presence of secondary peaks.

#### Effects of the autocorrelation of common inputs

So far, we considered only the situation in which the activity in the common presynaptic network does not display correlations. If that activity display some amount of short-term temporal correlation, an important question is how far these correlations are transmitted to the two neurons receiving the common inputs. If the presynaptic activity is correlated on a timescale  $au_{\rm pre}$ , i.e., its autocorrelation is of the form  $A_0 \exp(-t/\tau_{pre})$ , these correlations will induce an additional timescale  $\tau_{\rm pre}$  in C(t). Figure 9 displays the cross-correlation function C(t) obtained for two values of  $\tau_{pre}$ compared with C(t) obtained from asynchronous inputs. If  $\tau_{pre}$  is shorter than the correlation time (maximum between synaptic decay timescale  $\tau_s$  and dominant neural timescale  $\tau_1$ , 4.5 ms in the case for parameters of Fig. 9), the cross-correlation function is essentially identical to the case of asynchronous inputs. If  $\tau_{\rm pre}$  is larger than max( $\tau_s$ , $\tau_1$ ), the decay timescale of C(t) is given by  $\tau_{pre}$ . Correlations in the presynaptic activity can therefore only broaden the CCF between the two neurons but not sharpen it.



**Figure 9.** Cross-correlation function C(t) resulting from partially synchronous common inputs. **A**, Autocorrelation function  $\exp(-t/\tau_{pre})$  of the common inputs to the two neurons, for three values of the correlation time  $\tau_{pre}$ . **B**, Resulting cross-correlation functions. Note that, for  $\tau_{pre} = 0$  and  $\tau_{pre} = 1$  ms, the cross-correlation functions are almost perfectly identical.

In summary, the cross-correlation function arising from common inputs is in general highly symmetric. This is an important distinction from the highly asymmetric cross-correlation function generated by a direct synaptic connection. However, if the firing rates of the two neurons differ significantly and the amplitude of background is low in at least one of the two neurons, the cross-correlation function arising from common inputs is asymmetric so that, in that case, asymmetry does not imply that a direct connection is present between the two neurons. The width and the amplitude of the cross-correlation function depend on the properties of the synapses mediating common inputs. The amplitude of the CCF is, however, modulated in a much stronger way by the firing statistics of the neurons, which are set by independent background inputs: for fixed amplitude of common inputs, the amplitude of the cross-correlations is much larger when the neurons fire regularly than when they fire irregularly.

#### Other simple microcircuits

The knowledge of the cross-correlation functions for the two cases of directly connected neurons and neurons receiving common inputs provides us with the basic tools for calculating the cross-correlation function in more complex circuits. Within the linear approximation, any circuit can be decomposed in a superposition of simpler ones, and the cross-correlation function for that circuit can be obtained as a sum of cross-correlation functions of the simpler circuits. This approach is illustrated here on a couple of basic, experimentally relevant microcircuits.

#### Mutually connected neurons

The circuit, consisting of two neurons mutually connected by two synapses (Fig. 10*A*), is one of the connectivity patterns found to occur with high probability in the cortex (Markram et al., 1997; Sjöström et al., 2001; Song et al., 2005). A number of theoretical (Van Vreeswijk et al., 1994; Ernst et al., 1995; Lewis and Rinzel, 2003) studies have examined the activity in mutually coupled pairs of neurons, especially the synchronization properties between the two neurons in the case in which they fire regularly (low background synaptic noise).

The cross-correlation between the two neurons can be written as follows (Fig. 10*A*):

$$C(t) = C_{1 \to 2}(t) + C_{2 \to 1}(t), \qquad (31)$$

where  $C_{1\rightarrow 2}$  (resp.  $C_{2\rightarrow 1}$ ) is the cross-correlation of the monosynaptic circuit in which the neuron 1 projects a synapse on neuron 2 (resp. neuron 2 on neuron 1). If the two neurons are identical and receive identical background inputs, then  $C_{2\rightarrow 1}(t) = C_{1\rightarrow 2}(-t)$ . Here we only examine the case of high background synaptic noise. This will allow us to determine how far the main findings of previous, low-noise, studies extend to high noise. We moreover assume that the synaptic reversal potential  $E_{syn}$  is significantly different from the mean membrane potential of the two neurons, so that synaptic inputs are dominated by current inputs.

Previous studies have found that the delay in synaptic transmission plays a key role in synchronizing the two neurons (Ernst et al., 1995). If  $C_{1\rightarrow2,0}(t)$  is the cross-correlation function for a single synaptic connection without delay, the

cross-correlation function  $C_{\delta_s}(t)$  for two mutually coupled neurons with a synaptic delay  $\delta_s$  is given by the following:

$$C_{\delta_s}(t) = C_{1 \to 2,0}(t - \delta_s) + C_{1 \to 2,0}(-t + \delta_s).$$
(32)

Figure 10*B* displays the cross-correlation function as the delay is increased, for the case of inhibitory synapses. In absence of synaptic delay, inhibitory coupling induces strong anti-correlations at short times, but at zero lag the cross-correlation is equal to zero, i.e., no synchrony is present. For a synaptic delay of 1 ms, the inhibitory anti-correlations persist, but positive correlations appear at zero time lag so that the synchronization of the two neurons is increased. This increase is attributable to the disinhibition caused by the effective refractory period at negative times in  $C_{1\rightarrow2,0}(t)$  (Fig. 5). If the synaptic delay is further increased to 5 ms, the maximum of  $C_{\delta_s}(t)$  shifts away from zero, so that the coupling does not promote zero lag synchrony anymore. Our results therefore confirm the role of synaptic delays in the synchronization of two mutually coupled neurons, even for high background noise.

Another striking result of low-noise studies is that inhibitory synapses between mutually coupled neurons promote synchrony, whereas excitatory synapses instead promote antisynchrony (Van Vreeswijk et al., 1994; Ernst et al., 1995). Within our linear approximation in the regime of current-dominated synaptic interactions, the cross-correlation function  $C_{\delta_i}^{(e)}(t)$  for neurons coupled by excitatory synapses is simply obtained as  $C_{\delta_i}(t) = -C_{\delta_i}^{(i)}(t)$ , where  $C_{\delta_i}^{(i)}(t)$  is the cross-correlation function for neurons coupled by inhibitory synapses. It is thus immediately clear that, whereas inhibition induces zero-lag correlations and anti-correlations at small times, excitation instead leads to anti-correlations at zero lag and positive correlations at small times, i.e., out-of-phase synchrony.

# Feedforward inhibition

It has been experimentally observed that inhibitory and excitatory inputs to neurons are often not independent but instead co-occur with a precise timing (Pouille and Scanziani, 2001; Wehr and Zador, 2003; Brunel et al., 2004; Mittmann, 2005). Such a coordination of excitatory and inhibitory inputs can be implemented via feedforward inhibition. In this simple microcircuit, illustrated in Figure 11, common excitatory inputs arrive on neuron 1, an inhibitory interneuron, and neuron 2. Neuron 2 also receives direct synaptic inputs from neuron 1. Neuron 2 thus receives excitatory inputs, closely followed by inhibitory inputs elicited by excitation in neuron 1. The cross-correlation function C(t) for feedforward inhibition can be obtained as the sum of



**Figure 10.** Cross-correlation function C(t) for two mutually coupled LIF neurons. **A**, The cross-correlation function of the full circuit is obtained as the sum of the cross-correlation functions of two simpler circuits. In this example, the synapses are excitatory, and the synaptic delay is 1 ms. **B**, C(t) in the case of inhibitory synapses, as the synaptic delay time is increased. In both panels, the two neurons fire at 30 Hz and receive moderate background synaptic noise ( $\sigma = 6$  mV), and the PSC peak amplitude is 100 pA. Histograms show results of direct numerical simulations.



**Figure 11.** Cross-correlation function C(t) for feedforward inhibition. The cross-correlation function of the full circuit is obtained as the sum of the cross-correlation functions of two simpler circuits. For comparison, the histogram shows results of direct numerical simulations. Both neurons are LIF neurons firing at 30 Hz, and the amplitude of background synaptic noise is  $\sigma = 6$  mV. The PSC amplitudes are 100 and 150 pA for the synaptic connection and the common inputs, respectively.

cross-correlations arising from common inputs and crosscorrelations arising from a direct synaptic connection. It should be noted that the cross-correlation function depends linearly on the inhibitory synaptic weight but quadratically on the excitatory weights. The precise shape of the cross-correlation function is thus not simply scaled by the input strengths but depend on their relative weights. Figure 11 illustrates the shape of the crosscorrelation function for feedforward inhibition in the case of strong background synaptic noise in both neurons. The common inputs lead to a broad central peak in C(t), which is truncated by the inhibition, thus improving the precision of synchrony between the two neurons. A cross-correlogram with the same characteristic shape has been recently obtained from *in vivo* recordings in a cerebellar circuit identified as potential feedforward inhibition by *in vitro* studies (Léna et al., 2008).

# Discussion

The aim of this study was to examine the relation between the CCF of two neural spike trains and the underlying connectivity, synaptic properties, and firing statistics of the two neurons. To this end, we used integrate-and-fire models of neurons that incorporate some of the essential biophysical properties of real neurons but remain simple enough to be fully analyzed mathematically. We explicitly modeled two neurons only and took into account the activity of the surrounding network, which we assumed to be stationary, as a fluctuating background input that sets each of the neurons in a baseline state with a nonzero firing rate. The response properties to synaptic inputs in this baseline state can be determined analytically and give access to the CCFs within a linear approximation (Brunel and Hakim, 1999; Brunel, 2000; Lindner and Schimansky-Geier, 2001; Lindner et al., 2005; Richardson, 2007). This approximation remains accurate for cross-correlations of amplitude up to 0.3. We therefore expect it to be relevant for the strong background noise usually observed *in vivo* (Anderson et al., 2000). Using this approach, we determined the CCFs for different patterns of connectivity, starting with the case of a direct synaptic connection from one neuron to the other and the case of common inputs to the two neurons. We then showed how the results for these two simple circuits can be exploited to study the CCF in more complex situations.

## Modulating the functional interactions

The functional interactions between two neurons, as quantified by the CCF between their spike trains, depend in an essential manner on the properties of the synapses providing the inputs. In a first approximation, the amplitude of the CCF is proportional to the peak PSC in the case of a direct synaptic connection and to its square in the case of common inputs so that plastic modifications of synaptic strength obviously modulate functional interactions. The full time course of the CCF is determined by a temporal filtering of the PSC by the firing response of the postsynaptic neuron(s). The properties of this firing response however depend on the statistics of baseline firing of the postsynaptic neuron(s).

The amplitude and shape of functional interactions are therefore not set by the synaptic properties alone but strongly depend on the background synaptic inputs to the postsynaptic neuron(s), i.e., the activity of the surrounding network, which determines their firing statistics. If the fluctuations in background inputs are weak and the firing of the postsynaptic neuron regular, additional synaptic inputs have a much larger effect than if the background fluctuations are strong and the firing of that neuron very irregular. As a consequence, for a fixed PSC amplitude, the amplitude of the CCF varies in a highly nonlinear manner with the strength of background noise, in agreement with previous observations (Poliakov et al., 1996). Changes of the firing regularity by background inputs modulates the functional interactions in a much stronger and flexible manner than plastic modifications of synaptic weights. Thus, background noise affects both the gain of neurons (Chance et al., 2002), i.e., their steady-state direct current response, and their correlations that are determined by their response at intermediate frequencies.

#### Reading out the connectivity

An important question is whether the CCF can be used to distinguish monosynaptically connected neurons from neurons receiving common inputs. For two identical neurons firing with identical statistics, the CCF is highly asymmetric in the former case, although it is perfectly symmetric in the latter case. Symmetry has therefore been commonly used as a criterion to distinguish between the two situations (Alonso and Martinez, 1998; Fujisawa et al., 2008). It was, however, a priori not clear how accurate this criterion would remain for two neurons with very different intrinsic properties or firing statistics, because such heterogeneities disrupt the symmetry of the CCF in response to common inputs. We found that, even for high degrees of heterogeneity between the two neurons, in the case of strong background fluctuations, the asymmetry remains much weaker in the case of common inputs than for a direct synaptic connection. In contrast, for low background noise, the CCF arising from common inputs can be highly asymmetric. The symmetry is therefore a robust criterion for distinguishing a direct synaptic connection from common inputs only in the case of strong background noise.

In large recurrent networks, two neurons that are part of the same network receive common input from the network that can potentially have a nontrivial temporal structure as a result of the collective network dynamics (Brunel and Hakim, 1999; Brunel, 2000). In this situation, an interesting question is whether the cross-correlation is dominated by the collective dynamics of the network (making identification of synaptic connectivity difficult if not impossible) or by the direct (monodirectional or bidirectional) synaptic connection. For networks of binary neurons, Ginzburg and Sompolinsky (1994) showed that, if the network is in an asynchronous state and far from bifurcations leading to synchronized states, cross-correlations can be dominated by direct connections, whereas close to such bifurcations the effect of direct connections is very small compared with the collective dynamics of the network. For more realistic networks of spiking neurons, cross-correlations have been studied analytically only in extremely simplified architectures [homogeneous and fully connected networks (Meyer and Van Vreeswijk, 2002)] or through numerical simulations (Amit and Brunel, 1997). The question of the relative impact of direct connections and collective dynamics on cross-correlations therefore remains an open issue in realistic networks of spiking neurons.

#### Comparison with previous studies

Previous theoretical studies have examined separately the crosscorrelations in the case of a direct synaptic connection (Knox, 1974; Ashby and Zilm, 1982; Fetz and Gustafsson, 1983; Poliakov et al., 1996, 1997; Herrmann and Gerstner, 2001, 2002) and common inputs (de la Rocha et al., 2007; Shea-Brown et al., 2008; Tchumatchenko et al., 2008). Here, we have developed a common framework for these two and other circuits and systematically included the effects of the surrounding network by taking into account background synaptic inputs to the neurons. For a direct synaptic connection, our approach is similar in spirit to the study of Herrmann and Gerstner (2001). These authors also made use of linear response, but they modeled background synaptic inputs as "escape" noise instead of diffusion noise in our work. For the case of common inputs, our approach is also closely related to the one adopted by de la Rocha et al. (2007) and Shea-Brown et al. (2008) to study spike-count correlations. However, the spike-count correlation of two spike trains is related to the time integral of the CCF (Bair et al., 2001) and therefore different from the amplitude of the CCF (Kohn and Smith, 2005). Moreover, different normalizations are commonly used for the two quantities (see Materials and Methods). Although spike-count correlations arising from common inputs depend on the firing rate of the neurons, they were found to be insensitive to the regularity of the firing (de la Rocha et al., 2007), in contrast to our results for the CCFs.

For the situation of a direct synaptic connection, the previous studies (Knox, 1974; Ashby and Zilm, 1982; Fetz and Gustafsson, 1983; Poliakov et al., 1996, 1997; Herrmann and Gerstner, 2001, 2002) have sought to relate the postsynaptic potential to the CCF, and it has been debated whether the PSP, its time derivative, or a combination of the two determine the shape of the CCF. The reason to consider the PSP (or its derivative) rather than the PSC, as we do, was that, in the absence of background synaptic inputs, the PSP determines when the membrane potential crosses the threshold. In the presence of background synaptic inputs, a probabilistic reasoning becomes necessary, and we find it more natural to express the CCF in terms of the PSC shape rather than PSP. Because the PSP is obtained by the filtering of the PSC through the membrane, our results are not in conflict with previous observation that both the PSP and its time derivative have an influence on the CCF.

#### Interpreting experimental data

The present results should be helpful for the interpretation of experimental results. Here, we do not attempt to provide an exhaustive survey of the literature but instead point out a couple of examples. In an impressive recent study, Fujisawa et al. (2008) were able to track the variations of CCF between neurons from the prefrontal cortex of the rat, at different epochs of a working memory task. They observed strong modulations of the CCF amplitude and interpreted them as evidence of shortterm plasticity. Our results suggest that, alternatively, such modulations may result from modulations of the firing regularity of the postsynaptic neuron, arising from changes in background inputs from the surrounding network. The present analysis, however, assumed stationary background inputs, and the implications of the variation of background inputs certainly deserves additional examination. In another study (Csicsvari et al., 1998), strong cross-correlations were observed on the timescale of 1 ms. Our results, which relate the neuronal and synaptic timescales to the timescales of the CCF, suggest that extremely fast neuronal and synaptic timescales underlie such fast correlations. A number of other experimental studies have observed cross-correlations at timescales significantly longer that the synaptic and neural timescales (Kohn and Smith, 2005). These long timescales could arise from either intrinsic neuronal currents acting on slow timescales, such as firing rate adaptation, or slow dynamics of a network projecting to both recorded neurons.

Finally, several recent theoretical studies have focused on reproducing quantitatively the precise time course of arbitrary CCFs (Rosenberg et al., 1998; Truccolo et al., 2004). Powerful methods, based on the framework of point processes, are now available to fit models to experimental CCFs (Pillow et al., 2008) and extract effective parameters for neuronal interactions. However, these effective parameters do not have a direct biophysical interpretation and are not directly linked to the underlying circuitry. It would thus be interesting to combine the tools developed for statistical inference with the present analytical results to extract biophysically constrained parameters from the fitting of models to experimental data.

# Appendices

## Appendix A: linear response to synaptic inputs

In this section, we calculate the linear response of the firing rate to a variation g(t) of the synaptic conductance.

The dynamics of the membrane potential of the postsynaptic cell are given by the following:

$$c_m \frac{dV}{dt} = -g_m V + g_m \psi(V) + I_0 + \sigma \sqrt{c_m g_m} \eta(t) - g(t)(V - E_{\rm syn}). \quad (33)$$

We divide both sides by  $g_m + g(t)$ , write  $\delta g = g(t)/g_m$ , and keep only first-order terms in  $\delta g$ , so that Equation 33 becomes the following:

$$\tau_m (1 - \delta_g) \frac{dV}{dt} = -V + (1 - \delta_g)\psi + (1 - \delta_g)\mu + \left(1 - \frac{1}{2}\delta_g\right)\sigma \sqrt{\tau_m (1 - \delta_g)}\eta(t) + \delta_g E_{\text{syn}}, \quad (34)$$

where  $\tau_m = c_m/g_m$  is the membrane time constant, and  $\mu = I_0/g_m$  represents the effective rest value that the membrane potential would reach in absence of threshold. Equation 34 can be seen as a perturbed version of the following equation:

$$\tau_m \frac{dV}{dt} = -V + \psi + \mu + \sigma \sqrt{\tau_m} \eta(t), \qquad (35)$$

with the parameters  $\tau_m$ ,  $\mu$ ,  $\sigma^2$ , and  $V_T$  (in the EIF model only) being perturbed to values  $\tau_m(1 - \delta g)$ ,  $\mu(1 - \delta g) + \delta g(t) E_{syn}$ ,  $\sigma^2(1 - \delta g)$ , and  $V_T + \Delta_T \delta g$ , respectively.

In absence of the perturbation corresponding to synaptic inputs, the inputs in Equation 35 are constant and lead to a stationary firing  $\nu_0 = F(\mu, \sigma)$ , *F* being the transfer (or *f*–*I* curve) function, which can be calculated analytically (Tuckwell, 1988). The presence of a time-varying perturbation leads to a temporal variation of the firing rate, which on the linear level can be written as follows:

$$\nu(t) = \nu_0 + \int_0^\infty R_n(\tau) g(t-\tau) d\tau$$
 (36)

or in frequency

$$\tilde{\nu}(\omega) = 2\pi\nu_0\delta(\omega) + \tilde{R}_n(\omega)\tilde{g}(\omega), \qquad (37)$$

where  $\tilde{R}_n(\omega)$  is the Fourier transform of the linear response kernel, and  $\tilde{g}(\omega)$  is the Fourier transform of the synaptic conductance g(t).

From Equation 34, it is apparent that the linear response to a synaptic conductance change can be expressed as the sum of linear responses to the varied parameters as follows:

$$\tilde{R}_{n}(\omega) = (E_{\text{syn}} - \mu)\tilde{R}_{\text{E}}(\omega) - \sigma^{2}\tilde{R}_{\sigma^{2}}(\omega) - \tau_{m}\tilde{R}_{\tau_{m}}(\omega) + \Delta_{\text{T}}\tilde{R}_{V_{\text{T}}}(\omega), \quad (38)$$

where  $\tilde{R}_{\rm E}$ ,  $\tilde{R}_{\sigma^2}$ ,  $\tilde{R}_{\tau_m}$ , and  $\tilde{R}_{V_{\rm T}}$  are the linear responses in frequency of the firing rate to variations of parameters  $\mu$ ,  $\sigma^2$ ,  $\tau_m$ , and  $V_{\rm T}$  (EIF model only), each divided by  $g_m$  with the chosen normalization.

The linear response functions to variations of any parameter in Equation 35 have been analyzed in previous studies using the Fokker–Planck equation. In particular,  $\tilde{R}_E$  is the response to the variation of the external input current (Brunel and Hakim, 1999; Brunel et al., 2001). For the LIF model,  $\tilde{R}_E$  and  $\tilde{R}_{\sigma^2}$  can be expressed explicitly (Brunel and Hakim, 1999; Brunel et al., 2001; Lindner and Schimansky-Geier, 2001):

$$\tilde{R}_{\rm E}(\omega) = \frac{\nu_0}{g_m \sigma (1 + i\omega\tau_m)} \frac{\frac{\partial u}{\partial y}(y_{\rm T}, \omega) - \frac{\partial u}{\partial y}(y_{\rm R}, \omega)}{u(y_{\rm T}, \omega) - u(y_{\rm R}, \omega)}$$
(39)

and

$$\tilde{R}_{\sigma^2}(\omega) = \frac{\nu_0}{2g_m \sigma^2 (2 + i\omega\tau_m)} \frac{\frac{\partial^2 u}{\partial y^2} (y_{\rm T}, \omega) - \frac{\partial^2 u}{\partial y^2} (y_{\rm R}, \omega)}{(u(y_{\rm T}, \omega) - u(y_{\rm R}, \omega))},$$
(40)

where  $y_{\rm T} = (V_{\rm th} - I_0)/\sigma$ ,  $y_{\rm R} = (V_{\rm r} - I_0)/\sigma$ , and  $u(y,\omega)$  is given in terms of a combination of hypergeometric functions or equivalently as the solution of the following differential equation:

$$\frac{d^2u}{dy^2} = 2y\frac{du}{dy} + 2i\omega\tau_m u,$$
(41)

with the condition that *u* is bounded as  $y \rightarrow -\infty$ .

Note that the amplitude of  $\tilde{R}_{\rm E}$  decays asymptotically to zero as  $1/\sqrt{\omega}$ , so that  $\tilde{R}_{\rm E}$  is a low-pass filter. In contrast,  $\tilde{R}_{\sigma^2}$  converges to a nonvanishing constant, so that fast variations of the noise variance are transmitted instantaneously by the neuronal firing rate, a property studied by Lindner and Schimansky-Geier (2001) and Silberberg et al. (2004).

The response  $\hat{R}_{\tau_m}$  to the variation of the membrane timescale is simply a constant (for both LIF and EIF models) (Richardson, 2007):

$$\tilde{R}_{\tau_m}(\omega) = -\frac{\nu_0}{g_m \tau_m} \,. \tag{42}$$

Any temporal variation of the membrane time constant is thus perfectly reproduced by the temporal variation of the firing rate.

For the EIF model, the response functions  $\tilde{R}_{\rm E}$ ,  $\tilde{R}_{\sigma^2}$ , and  $\tilde{R}_{V_{\rm T}}$  have been studied by Richardson (2007), in which an efficient semi-numerical method based on the Fokker–Planck equation was developed to evaluate the response  $\tilde{R}_{\alpha}$  to the variation of any parameter  $\alpha$  as follows:

$$\tilde{R}_{\alpha} = \frac{j_{\alpha}}{j_{r}},\tag{43}$$

where the function  $j_r$  in the denominator is independent of the varied parameter  $\alpha$ . We used the same method in this study. Note that, for the EIF model,  $\tilde{R}_E$  is a low-pass filter, the amplitude of which decays as  $1/\omega$ . In contrast to the LIF model,  $\tilde{R}_{\sigma^2}$  is also a low-pass filter, with an amplitude also decreasing as  $1/\omega$ .  $\tilde{R}_{V_T}$  is, however, a high-pass filter, privileging fast variations of  $V_T$ .

Note that  $\tilde{R}_n$  can be written as follows:

$$\tilde{R}_n = (E_{\rm syn} - \mu)\tilde{R}_{\rm E} + \tilde{R}_{\rm shunt},\tag{44}$$

where

$$\tilde{R}_{\rm shunt}(\omega) = -\sigma^2 \tilde{R}_{\sigma^2}(\omega) - \tau_m \tilde{R}_{\tau_m}(\omega) + \Delta_{\rm T} \tilde{R}_{V_{\rm T}}(\omega) \qquad (45)$$

is independent of  $E_{syn}$  and corresponds to the shunting part of the synaptic conductance variation (for the LIF model,  $\Delta_T = 0$ ).

As a consequence, if the synaptic reversal potential is sufficiently different from the mean membrane potential  $\mu$ , the response to synaptic inputs is dominated by the response to the input current variation. In contrast, if  $E_{syn} = \sim \mu$ , the response to synaptic inputs is dominated by the response to the variation of the membrane conductance.

# Appendix B: relation between the response function and the spike-triggered average current

The linear response function to an input current  $R_{\rm E}$  is closely related to the STA current. It is not, however, fully equivalent to the Wiener kernel and STA current studied previously (Poliakov et al., 1997; Paninski, 2006). Here we describe explicitly this relation.

Consider a neuron that receives a mean input current and two time-varying inputs with flat power spectrum:

$$c_m \frac{dV}{dt} = -g_m V + g_m \psi(V) + I_0 + \sigma_v \sqrt{c_m g_m} \eta(t) + \sigma_s \sqrt{c_m g_m} \eta_s(t).$$
(46)

The first white-noise input  $\eta(t)$  represents background noise and is different in each trial. The second white noise-input  $\eta_s(t)$  has a flat power spectrum, but its time course is identical in each trial so that it represents the signal the neuron receives.

If the amplitude  $\sigma_s$  of the signal is small, and the variation of the firing rate (averaged over trials or equivalently background noise) around its mean  $\nu_0$  is given by the convolution with the response function  $R_{\rm E}$ :

$$\nu(t) = \nu_0 + \int_0^\infty \sqrt{c_m g_m} R_{\rm E}(\tau) \sigma_s \eta_s(t-\tau) d\tau.$$
 (47)

The linear response function  $R_{\rm E}$  is the optimal Wiener kernel in the presence of a background noise of amplitude  $\sigma$  and therefore corresponds to the spike-triggered average signal current. The cases studied by Poliakov et al. (1997) and Paninski (2006) correspond to the situation in which background noise is absent, so that all the time-varying input corresponds to the signal.

#### Appendix C: dominant timescale approximation for $R_n$

The linear response function  $\tilde{R}_n(\omega)$  is an analytic function. We call  $\zeta$  the analytical extension of  $\tilde{R}_n$ , defined by its values on the imaginary axis:

$$\zeta(i\omega) = \tilde{R}_n(\omega). \tag{48}$$

The complex function  $\zeta$  possesses a set of simple poles  $\{z_j\}_{j>0}$ , with  $\forall j, Re(z_j) < 0$ , and labeled such that  $Re(z_{j1}) < Re(z_{j2})$  if  $j_1 < j_2$ . These poles are the zeros of the denominator of  $\tilde{R}_n$ , i.e., the zeros of  $u(y_T) - u(y_R)$  (see Eq. 40) in the case of the LIF model and the zeros of  $j_r$  (see Eq. 43) in the case of the EIF model. Note that  $\tilde{R}_E$  and  $\tilde{R}_{shunt}$  have the same poles, so that the present analysis is not restricted to  $\tilde{R}_E$  alone.

The function  $\zeta$  can be written as an expansion over its poles:

$$\zeta(z) = \sum_{j=1}^{\infty} \frac{a_j}{z - z_j} + \text{ complex conj.,}$$
(49)

where  $a_i$  is the residue of  $\zeta$  at its *j*th pole.

Using Equation 49, the linear kernel  $R_n$ , the inverse Fourier transform of  $\tilde{R}_E$ , can be expressed as follows:

$$R_n(t) = \Theta(t) \sum_{j=1}^{\infty} a_j e^{z_j t} + \text{ complex conj.}, \qquad (50)$$

where  $\Theta(t) = 1$  if t > 0 and  $\Theta(t) = 0$  otherwise.

# Appendix D: calculation of cross-correlation functions

Direct synaptic connection

In the situation in which one neuron makes a direct synaptic connection on the other neuron, the dynamics of the membrane potentials of the presynaptic and postsynaptic neuron are given by the following:

$$c_m \frac{dV_{\rm pre}}{dt} = -g_m V_{\rm pre} + g_m \psi(V_{\rm pre}) + I_{\rm pre} + \sigma_{\rm pre} \sqrt{c_m g_m} \eta_{\rm pre}(t) \quad (51)$$

and

$$c_m \frac{dV_{\text{post}}}{dt} = -g_m V_{\text{post}} + g_m \psi(V_{\text{post}}) + I_{\text{post}} + \sigma_{\text{post}} \sqrt{c_m g_m} \eta_{\text{post}}(t) - g(t)(\text{pre}V - E_{\text{syn}}).$$
(52)

The postsynaptic conductance g(t) is given by the following:

$$g(t) = \int_{0}^{\infty} d\tau g_{\rm syn}(\tau) n_{\rm pre}(t-\tau), \qquad (53)$$

where  $n_{\text{pre}}$  is the train of spikes emitted by the presynaptic neuron, and  $g_{\text{syn}}$  is the postsynaptic conductance change attributable to a single presynaptic spike, defined in Equation 13.

We compute the cross-correlation function between the two neurons in a linear approximation in which the interaction between the two neurons is treated as a perturbation of the case when the two neurons are not connected. A similar approach was used previously by Lindner et al. (2005).

Within the linear approximation, the probability that the postsynaptic neuron spikes at time *t* can be written as follows:

$$\nu^{(\text{post})}(t) = \nu_{0,0}^{(\text{post})} + \int_{0}^{\infty} d\tau R_n(\tau) g(t-\tau), \qquad (54)$$

where  $\nu_{0,0}^{(\text{post})}$  is the firing rate that the postsynaptic neuron would have in the absence of the connection to the singled-out presynaptic neuron. The cross-correlation function between the spike trains of these two neurons is therefore as follows:

$$\langle n^{(\text{pre})}(t')n^{(\text{post})}(t)\rangle = \nu_0^{(\text{pre})}\nu_{0,0}^{(\text{post})} + \int_0^\infty d\tau R_n^{(\text{post})}(\tau)\langle n^{(\text{pre})}(t')g(t-\tau)\rangle.$$
(55)

Taking the Fourier transform with respect to both times t and t' gives the equivalent form in frequency as follows:

$$\langle \tilde{n}_{\text{pre}}^{*}(\omega')\tilde{n}_{\text{post}}(\omega) \rangle = (2\pi)^{2} \nu_{0}^{(\text{pre})} \nu_{0,0}^{(\text{post})} \delta(\omega) \delta(\omega') + \langle \tilde{n}_{\text{pre}}^{*}(\omega') \tilde{R}_{n}^{(\text{post})}(\omega) \tilde{g}(\omega) \rangle.$$
 (56)

From Equation 53, the Fourier transform of the conductance  $\tilde{g}(\omega)$  is proportional to the Fourier transform of the presynaptic spike train as follows:

$$\tilde{g}(\omega) = \tilde{g}_{\rm syn}(\omega)\tilde{n}_{\rm pre}(\omega),$$
 (57)

so that the following holds true:

$$\langle \tilde{n}_{\text{pre}}^{*}(\omega')\tilde{n}_{\text{post}}(\omega) \rangle = (2\pi)^{2} \nu_{0}^{(\text{pre})} \nu_{0,0}^{(\text{post})} \delta(\omega) \delta(\omega')$$
  
+  $\tilde{R}_{n}^{(\text{post})}(\omega) \tilde{g}_{\text{syn}}(\omega) \langle \tilde{n}_{\text{pre}}(\omega) \tilde{n}_{\text{pre}}^{*}(\omega') \rangle.$  (58)

One can express the averages on both sides of Equation 58 using the power spectrum of the presynaptic spike train,  $\tilde{A}_{pre}(\omega)$ , and the cross-spectrum between the presynaptic and postsynaptic neurons, as defined and normalized in Equations 9 and 11. We also note that the stationary firing rate of the postsynaptic neuron is modified when the singled-out presynaptic connection is taken into account and is given to linear order by the following:

$$\nu_0^{(\text{post})} = \nu_{0,0}^{(\text{post})} + \tilde{R}_n^{(\text{post})}(0)\tilde{g}_{\text{syn}}(0)\nu_0^{(\text{pre})}.$$
 (59)

Finally, we obtain the following:

$$\tilde{C}(\omega) = \frac{\nu_0^{(\text{pret})}}{\nu_0^{(\text{post})}} \tilde{R}_n^{(\text{post})}(\omega) \tilde{g}_{\text{syn}}(\omega) \tilde{A}_{\text{pre}}(\omega).$$
(60)

In the dominant timescale approximation,  $R_n = \frac{a_1 \tau_1}{1 + i\omega \tau_1}$ , and, for a Poisson presynaptic neuron, the cross-correlation function reads as follows:

$$C(t) = g_0 a_1 \frac{\tau_1 \tau_s}{\nu_0^{(\text{post})}(\tau_s - \tau_1)} \times (e^{-(t - \delta_s)/\tau_s} - e^{-(t - \delta_s)/\tau_1})\Theta(t - \delta_s). \quad (61)$$

Note that the maximum of C(t) in Equation 61 is as follows:

$$C_{\max} = g_0 a_1 \frac{\tau_s}{\nu_0^{(\text{post})}} \left(\frac{\tau_s}{\tau_1}\right)^{\frac{\tau_s}{\tau_1 - \tau_s}},\tag{62}$$

and occurs at the following:

$$t_{\max} = \frac{\tau_1 \tau_s}{\tau_s - \tau_1} \log\left(\frac{\tau_s}{\tau_1}\right) + \delta_s. \tag{63}$$

#### *Common inputs*

In the situation in which two neurons labeled 1 and 2 receive common inputs, the dynamics of the membrane potentials of the two neurons are given by the following:

$$c_m \frac{dV_i}{dt} = -g_m V_i + g_m \psi(V_i) + I_i + \sigma_i \sqrt{c_m g_m} \eta_i(t)$$
$$-g^{(i)}(t)(V - E_{\text{syn}}), \quad (64)$$

where i = 1, 2.

The conductance  $g^{(i)}$  of neuron *i* attributable to synaptic inputs from the common presynaptic network is given by the following:

$$g^{(i)}(t) = \int_{0}^{t} d\tau g^{(i)}_{\text{syn}}(\tau) n_{\text{pre}}(t-\tau), \quad i = 1, 2, \qquad (65)$$

where  $n_{\rm pre}$  is the spike train obtained by superposing the spike trains of all common presynaptic neurons. Here we assume that the synapses made by the presynaptic neurons are identical and simply depend on the postsynaptic neuron identity, but the derivation can be easily extended to a more general case.

Within the linear approximation, the firing probability of neuron i for a given presynaptic train  $n_{pre}$  can be written as follows:

$$\nu^{(i)}(t) = \nu_0^{(i)} + \int_0^{+\infty} d\tau R_n^{(i)}(\tau) [g^{(i)}(t-\tau) - \langle g^{(i)} \rangle], \quad (66)$$

where the average conductance  $\langle g^{(i)} \rangle$  attributable to the common presynaptic input has been substracted in the integral term so that  $\nu_0^{(i)}$  is the average firing rate of neuron *i*, arising from both the common inputs and the inputs specific to neuron *i*. Note also that, even for two identical neurons, the response functions  $R_n^{(1)}$  and  $R_n^{(2)}$  are different when the inputs  $(I_1,\sigma_1)$  and  $(I_2,\sigma_2)$  are different.

The correlation between the spike trains of neurons 1 and 2 is obtained by averaging over the common inputs as follows:

$$\langle \boldsymbol{\nu}^{(1)}(t) \boldsymbol{\nu}^{(2)}(t') \rangle = \boldsymbol{\nu}_{0}^{(1)} \boldsymbol{\nu}_{0}^{(2)}$$

$$+ \int_{0}^{+\infty} \int_{0}^{+\infty} d\tau d\tau' R_{n}^{(1)}(\tau) R_{n}^{(2)}(\tau') \langle [g^{(1)}(t-\tau) - \langle g^{(1)} \rangle]$$

$$\times [g^{(2)}(t'-\tau') - \langle g^{(2)} \rangle] \rangle$$
(67)

or equivalently

$$\langle [\nu^{(1)}(t) - \nu_{0}^{(1)}] [\nu^{(2)}(t') - \nu_{0}^{(2)}] \rangle$$
  
= 
$$\int_{0}^{+\infty} \int_{0}^{+\infty} d\tau d\tau' R_{n}^{(1)}(\tau) R_{n}^{(2)}(\tau') \langle [g^{(1)}(t - \tau) - \langle g^{(2)} \rangle] \rangle. \quad (68)$$

Moreover, the cross-correlation between the conductances of the two neurons can be related to the autocorrelation function of the common presynaptic spike train  $n_{\text{pre}}$  as follows:

$$\langle [g^{(1)}(s) - \langle g^{(1)} \rangle ] [g^{(2)}(s') - \langle g^{(2)} \rangle ] \rangle$$
  
=  $\int_{0}^{+\infty} \int_{0}^{+\infty} d\tau d\tau' g^{(1)}_{\text{syn}}(\tau) g^{(2)}_{\text{syn}}(\tau') \langle [n^{(\text{pre})}(s - \tau) - \nu_{0}^{(\text{pre})}] \rangle$   
 $\times [[n^{(\text{pre})}(s' - \tau') - \nu_{0}^{(\text{pre})}] \rangle$   
=  $(\nu_{0}^{(\text{pre})})^{2} \int_{0}^{+\infty} \int_{0}^{+\infty} d\tau d\tau' g^{(1)}_{\text{syn}}(\tau) g^{(2)}_{\text{syn}}(\tau') A_{\text{pre}}(s' - s + \tau - \tau').$  (69)

Finally, taking the Fourier transform of Equation 68 with respect to the time difference t' - t relates the cross-correlation function between the spike trains of neuron 1 and neuron 2 to the autocorrelation function of the common presynaptic spike train. With the normalization of Equation 9, it reads as follows:

$$\tilde{C}(\omega) = \frac{(\nu_0^{(\text{pre})})^2}{\nu_0^{(1)}\nu_0^{(2)}} \left(\tilde{R}_n^{(1)}(\omega)\tilde{g}_{\text{syn}}^{(1)}(\omega)\right)^* (\tilde{R}_n^{(2)}(\omega)\tilde{g}_{\text{syn}}^{(2)}(\omega))\tilde{A}_{\text{pre}}(\omega).$$
(70)

In the dominant timescale approximation,  $R_n = \frac{a_1 \tau_1}{1 + i\omega \tau_1}$ , and for identical neurons with asynchronous common inputs, the cross-correlation function reads as follows:

$$C(t) = g_0^2 a_1^2 \frac{\nu_0^{(\text{pret})}}{(\nu_0^{(\text{post})})^2} \frac{\tau_1^2 \tau_s^2}{2(\tau_s^2 - \tau_1^2)} (\tau_s e^{-|t|/\tau_s} - \tau_1 e^{-|t|/\tau|1}).$$
(71)

As a final remark, it can be noted that Equation 70 is quadratic in  $g_0$ . This might be a concern because we only computed the response to linear order. It can, however, be checked that quadratic terms in the response do not contribute to the cross-correlation function as defined here.

## Appendix E: power spectrum for the LIF model

The autocorrelation function can be deduced directly from the Fourier transform of the interspike interval distribution f(t) (Gerstner and Kistler, 2002). Indeed, if we denote by A(t) the full autocorrelation function, its positive part  $A_+(t) = \nu_0 A(t) \Theta(t)$  obeys the following:

$$A_{+}(t) = f(t) + \int_{0}^{\infty} ds f(s) A_{+}(t-s).$$
 (72)

Taking the Fourier transform, we have the following:

$$\tilde{A}_{+}(\omega) = \frac{\tilde{f}(\omega)}{1 - \tilde{f}(\omega)},\tag{73}$$

and as  $\tilde{A}(\omega) = (1 + 2Re(\tilde{A}_+(\omega)))/\nu_0$ ,

$$\langle \tilde{n}_{\rm pre} \tilde{n}^*_{\rm pre} \rangle = \nu_0 Re \left( \frac{1 + \tilde{f}(\omega)}{1 - \tilde{f}(\omega)} \right).$$
 (74)

The Fourier transform of the interspike interval distribution can be calculated analytically for the LIF neuron (Tuckwell, 1988), and it reads as follows:

$$\tilde{f}(\omega) = \frac{u(y_{\rm R}, \omega)}{u(y_{\rm T}, \omega)},\tag{75}$$

where *u* is the function defined by Equation 41.

In conclusion, the power spectrum of the LIF neuron is given by the following:

$$\langle \tilde{n}_{\rm pre} \tilde{n}_{\rm pre}^* \rangle = \nu_0 Re \left( \frac{u(y_{\rm T}, \, \omega) + u(y_{\rm R}, \, \omega)}{u(y_{\rm T}, \, \omega) - u(y_{\rm R}, \, \omega)} \right).$$
(76)

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